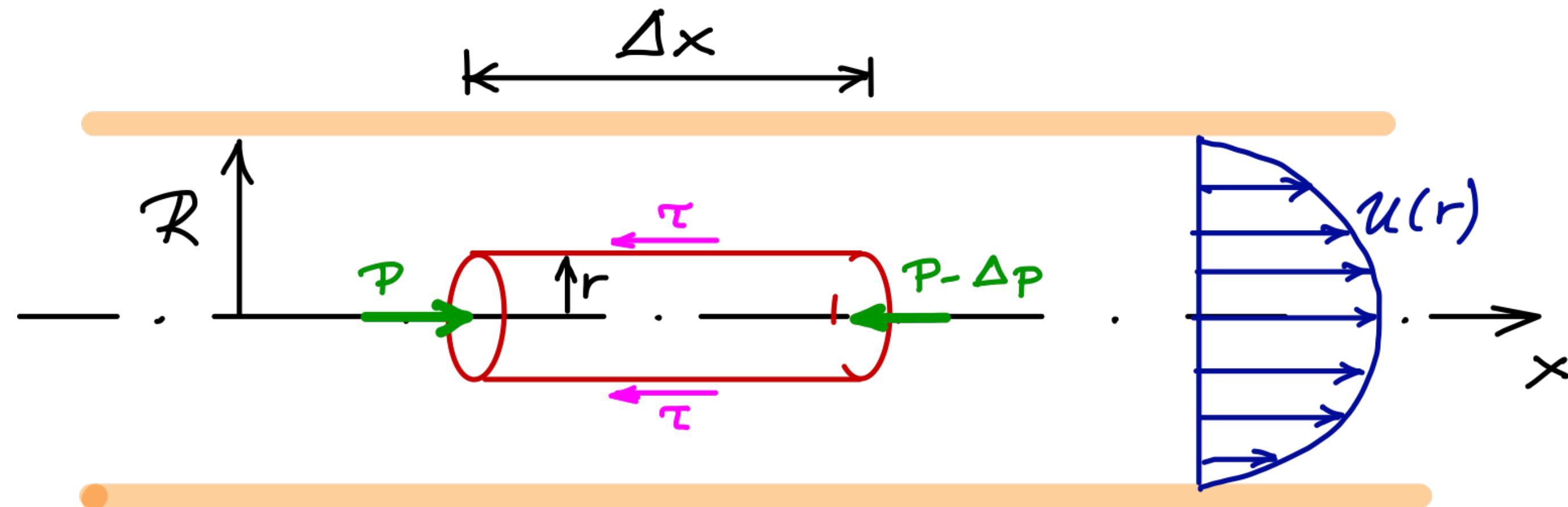


Poiseuille's law

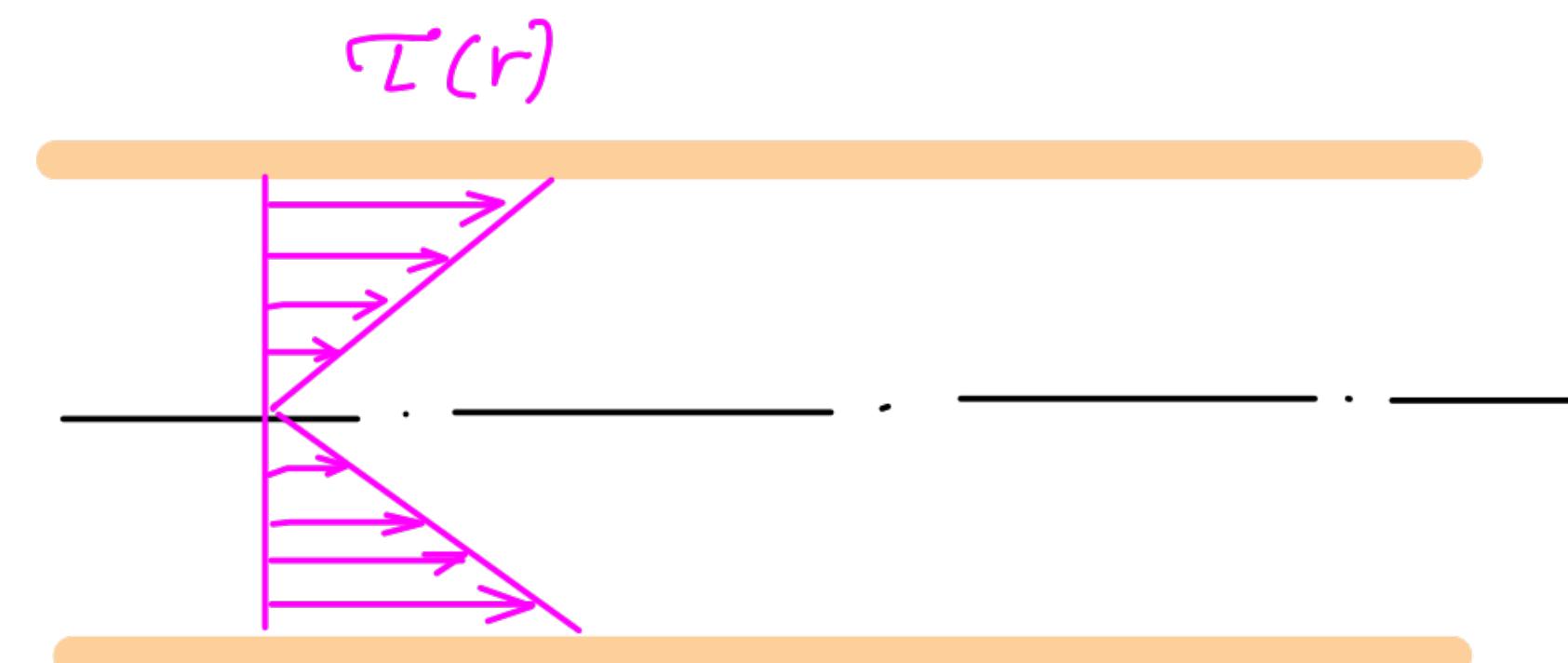


Newton's 2nd law: $\sum F_x = 0$

$$\Rightarrow P \cdot \pi r^2 - (P - \Delta P) \pi r^2 - 2\pi r \cdot \Delta x \cdot \tau = 0$$

$$\Rightarrow \Delta P \cdot \pi r^2 = 2\pi r \cdot \Delta x \cdot \tau$$

$$\Rightarrow \boxed{\tau = \frac{\Delta P}{\Delta x} \frac{r}{2}}$$



Maximum shear stress at the wall:

$$\boxed{\tau_w = \frac{\Delta P}{\Delta x} \frac{R}{2}}$$

Relation of pressure drop to velocity and flow (Hagen-Poiseuille law)

Assume Newtonian fluid: $T = -\mu \frac{\partial u}{\partial r}$

$$T = \frac{\Delta P}{\Delta x} \frac{r}{2} \Rightarrow -\mu \frac{\partial u}{\partial r} = \frac{\Delta P}{\Delta x} \frac{r}{2}$$

$$\Rightarrow \frac{\partial u}{\partial r} = -\frac{1}{2\mu} \frac{\Delta P}{\Delta x} r \Rightarrow \partial u = -\frac{1}{2\mu} \frac{\Delta P}{\Delta x} r \partial r$$

$$\Rightarrow u = -\frac{1}{4\mu} \frac{\Delta P}{\Delta x} r^2 + C$$

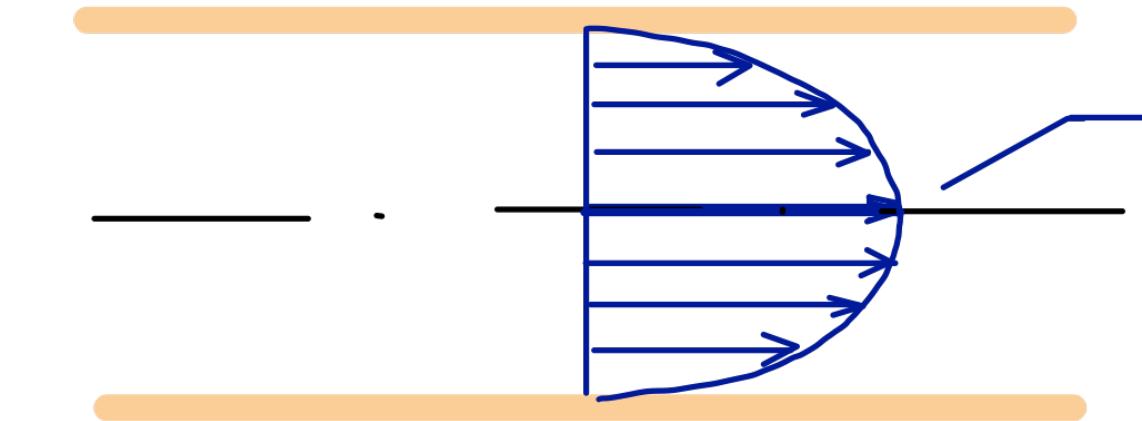
Boundary condition: $u=0$ for $r=R$

$$\therefore 0 = -\frac{1}{4\mu} \frac{\Delta P}{\Delta x} R^2 + C \Rightarrow C = \frac{1}{4\mu} \frac{\Delta P}{\Delta x} R^2$$

Hence,

$$u(r) = \frac{1}{4\mu} \frac{\Delta P}{\Delta x} (R^2 - r^2)$$

Parabolic profile



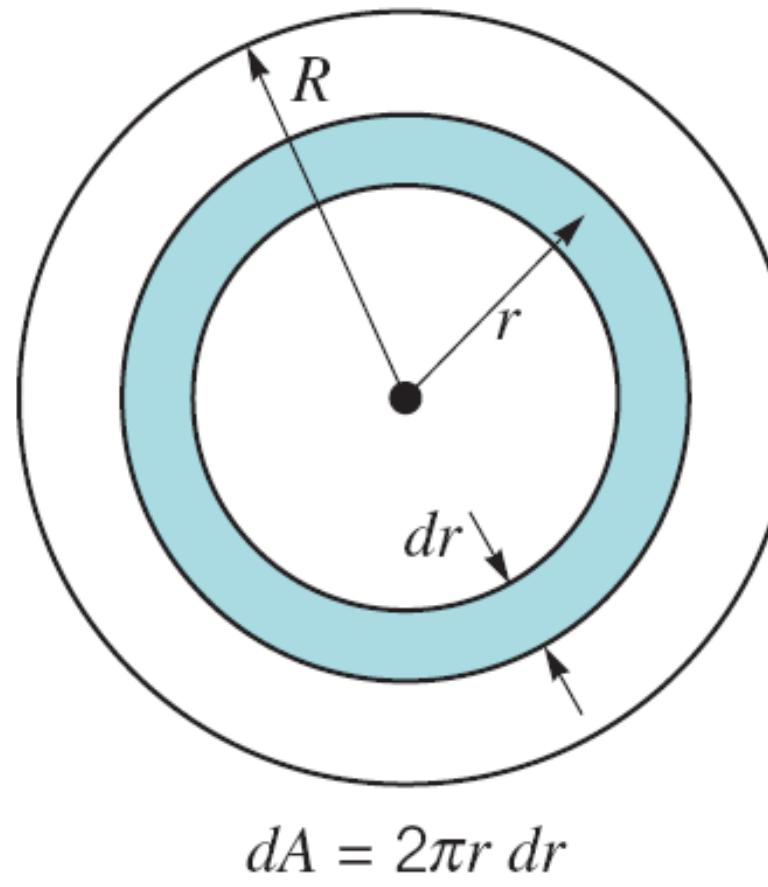
maximum Velocity

V_c @ $r=0$ (center)

$$V_c = \frac{1}{4\mu} \frac{\Delta P}{\Delta x} R^2$$

$$u(r) = V_c \cdot \left[1 - \frac{r^2}{R^2} \right]$$

Relation of pressure drop to velocity and flow (Hagen-Poiseuille law)



To get flow, Q , integrate over the cross section

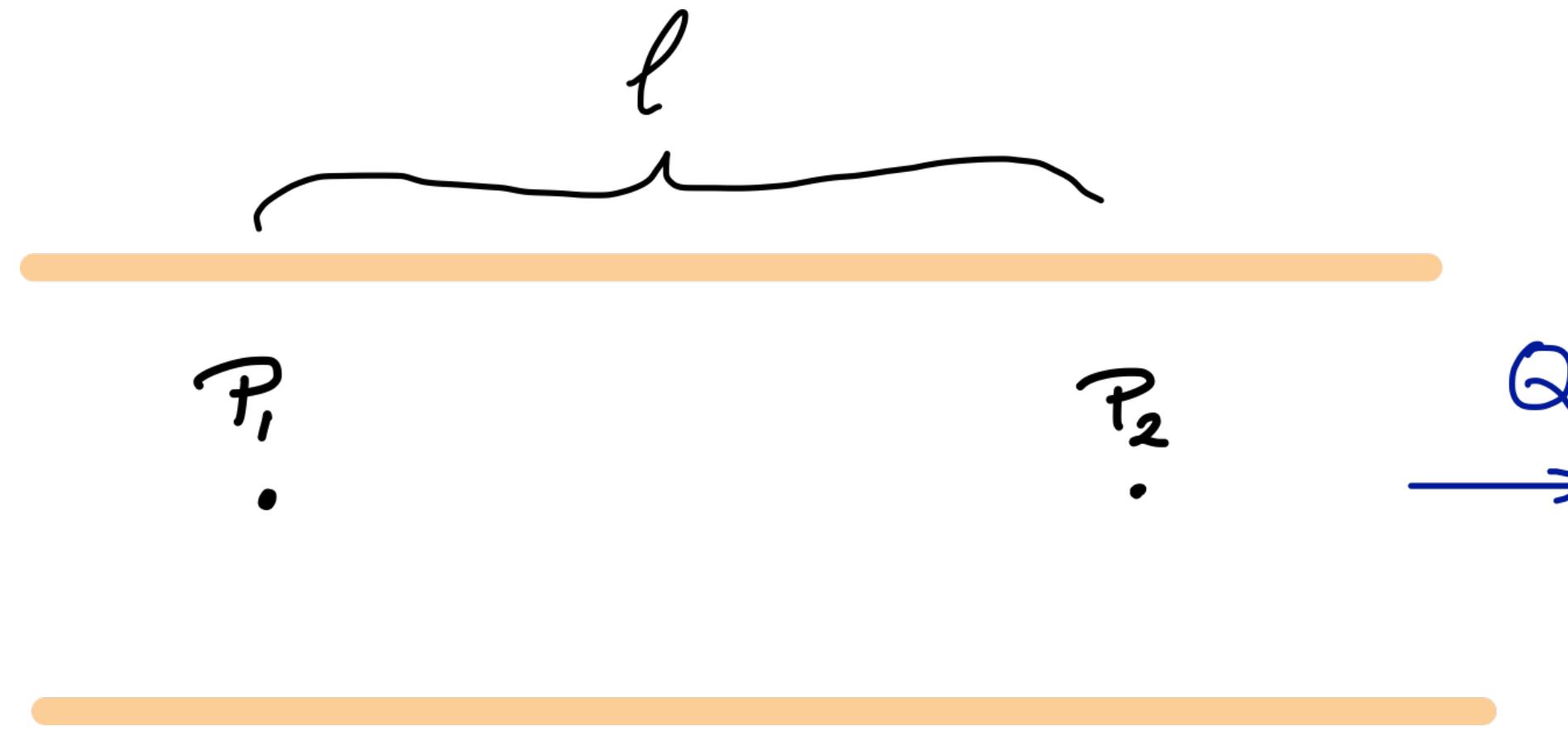
$$Q = \int_0^R u(r) 2\pi r dr = 2\pi V_c \int_0^R r \left[1 - \frac{r^2}{R^2} \right] dr$$

$$\Rightarrow Q = 2\pi V_c \int_0^R \left[r - \frac{r^3}{R^2} \right] dr = 2\pi V_c \left[\frac{r^2}{2} - \frac{r^4}{4R^2} \right]_0^R$$

$$Q = \frac{\pi R^2 V_c}{2} = \frac{\pi R^4}{8\mu} \frac{\Delta P}{\Delta x}$$

$$\text{Average velocity: } \bar{V} = \frac{Q}{\pi R^2} = \frac{V_c}{2}$$

Relation of pressure drop to velocity and flow (Hagen-Poiseuille law)



Note :

$$\underbrace{\frac{\Delta P}{\Delta x}}_{\text{pressure drop per unit length}} = - \underbrace{\frac{\partial P}{\partial x}}_{\text{pressure gradient}}$$

$$Q = \frac{\pi R^4}{8\mu l} \Delta P$$

or

$$\Delta P = \frac{8\mu l}{\pi R^4} Q$$

By analogy to Ohm's law:

$$\Delta P = \underbrace{\frac{8\mu l}{\pi R^4}}_{\text{Resistance}} Q$$

$$\begin{aligned} V &\rightarrow P \\ i &\rightarrow Q \\ R &\rightarrow R \end{aligned}$$

Wall shear stress for Poiseuille flow

$$\frac{\Delta P}{l} = \frac{2 \tau_w}{R} \Rightarrow \tau_w = \frac{\Delta P}{l} \frac{R}{2} = \left(\frac{8\mu}{\pi R^4} Q \right) \frac{R}{2} \Rightarrow \boxed{\tau_w = \frac{4\mu}{\pi R^3} Q}$$

Example Calculate the wall shear stress in the human abdominal aorta ($D = 12 \text{ mm}$; $\bar{Q} = 56 \text{ ml/s}$) and in external iliac artery ($D = 6.1 \text{ mm}$; $\bar{Q} = 6.8 \text{ ml/s}$).

Remark: In general, despite large variations in flow and diameter, τ_w is fairly constant across the arterial tree, with values in the range of 1.0 N/m^2 to 1.5 N/m^2

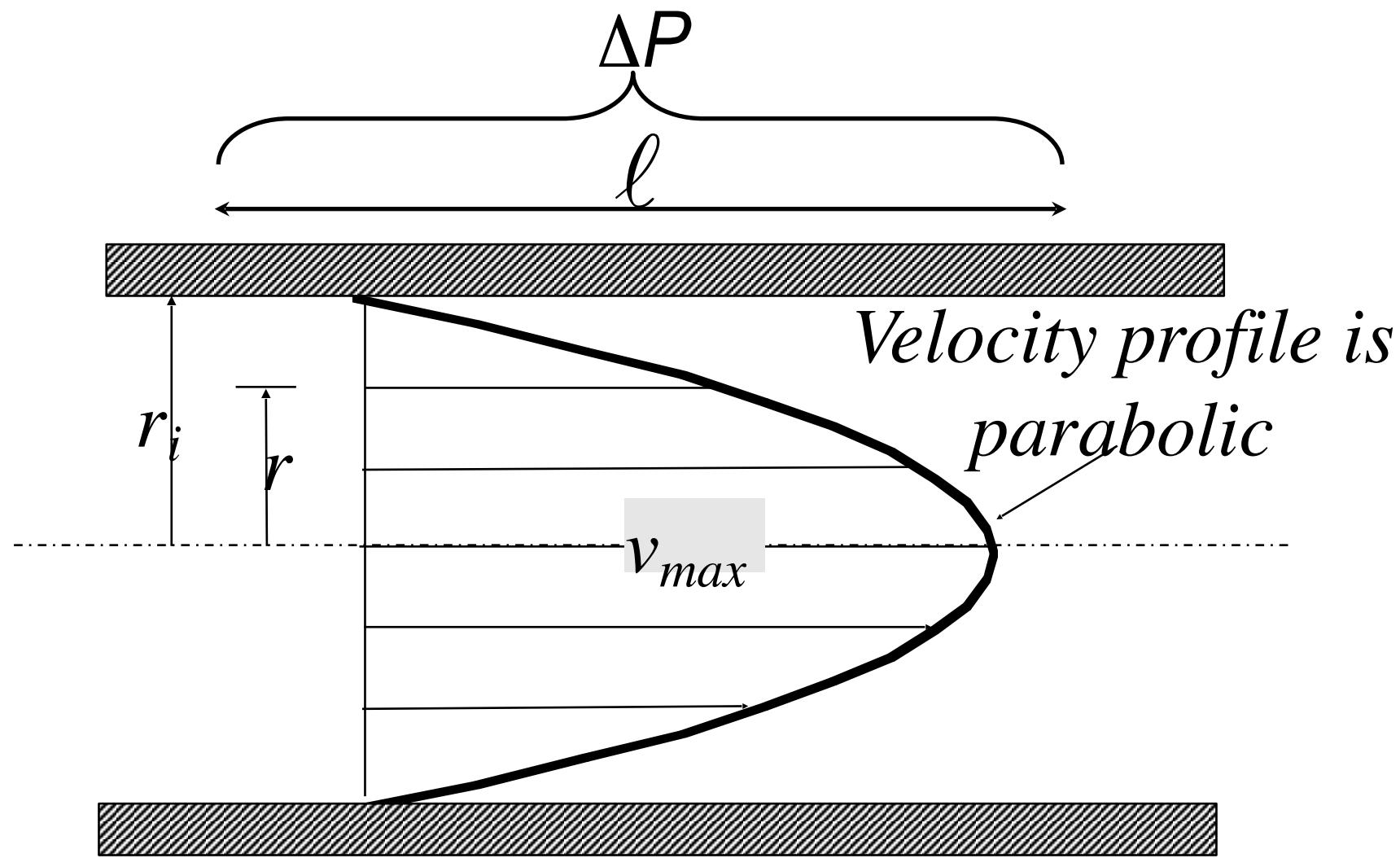
Abdominal aorta:

$$\tau_w = \frac{4 \cdot \mu}{\pi R^3} Q = \frac{4 \cdot 0.004 \text{ N.s/m}^2}{\pi \cdot 0.006^3 \text{ m}^3} \cdot 5.6 \times 10^{-5} \text{ m}^3/\text{s} \Rightarrow \boxed{\tau_w = 1.32 \text{ N/m}^2}$$

External iliac:

$$\tau_w = \frac{4 \cdot \mu}{\pi R^3} Q = \frac{4 \cdot 0.004 \text{ N.s/m}^2}{\pi \cdot 0.00305^3 \text{ m}^3} \cdot 6.8 \times 10^{-6} \text{ m}^3/\text{s} \Rightarrow \boxed{\tau_w = 1.23 \text{ N/m}^2}$$

Poiseuille's law: summary and limitations



$$v(r) = \frac{1}{4\mu} \frac{\Delta P}{\ell} (r_i^2 - r^2)$$

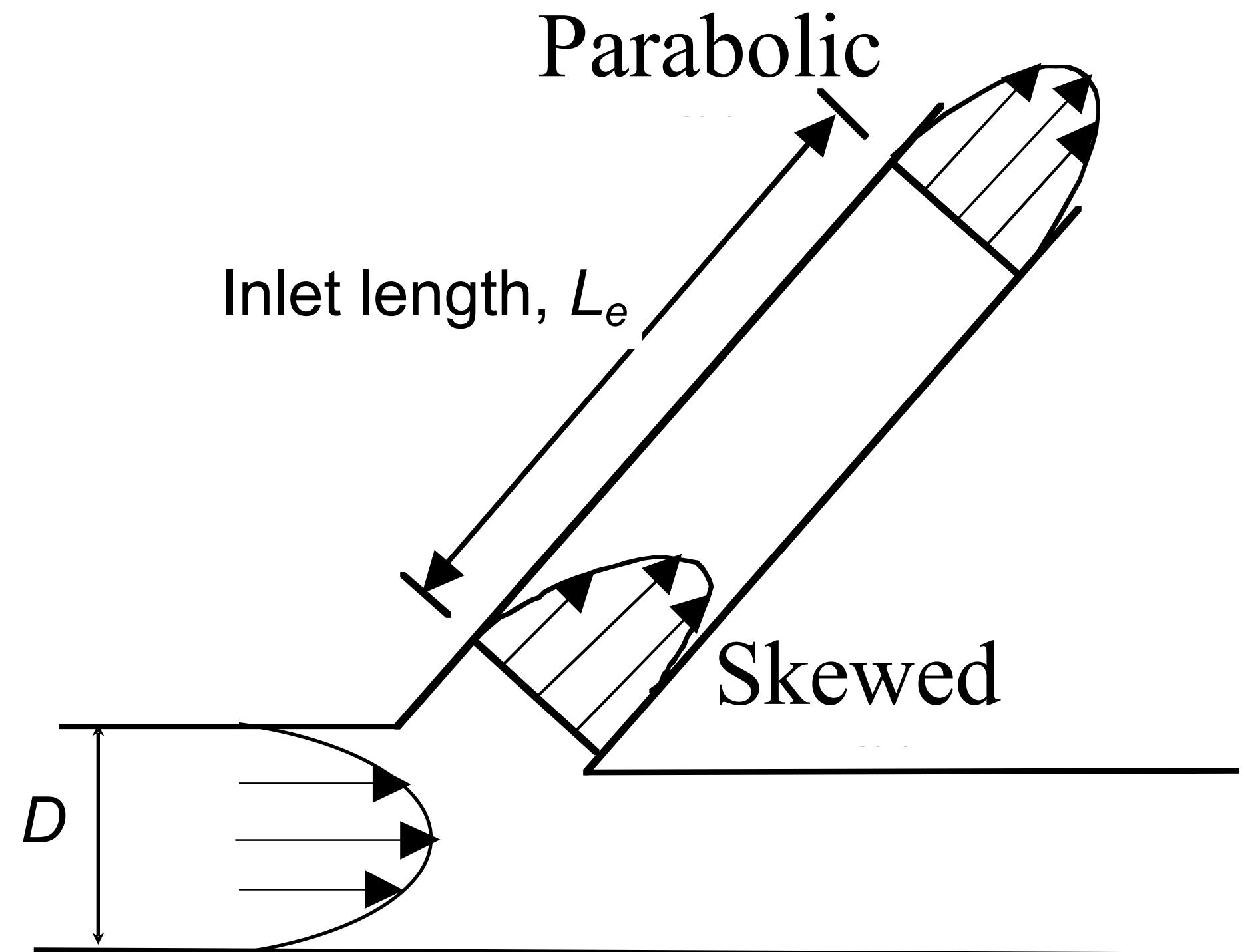
$$Q = \frac{\pi}{8\mu} \frac{\Delta P}{\ell} r_i^4$$

$$\tau = \frac{4\mu}{\pi r_i^3} Q$$

Conditions:

- Laminar, steady and developed flow
- Newtonian fluid
- Straight, uniform, constant diameter tube
- Rigid wall

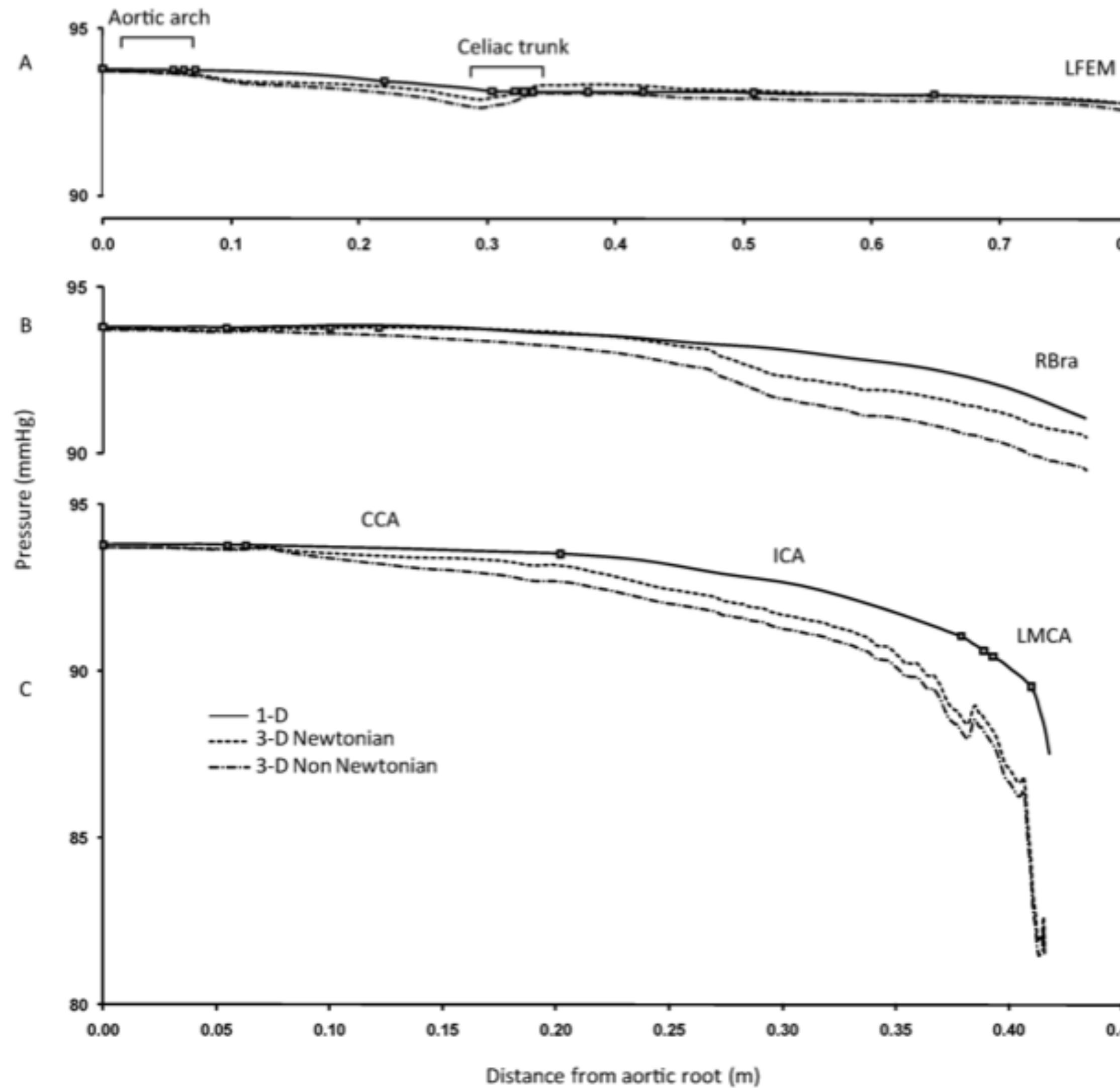
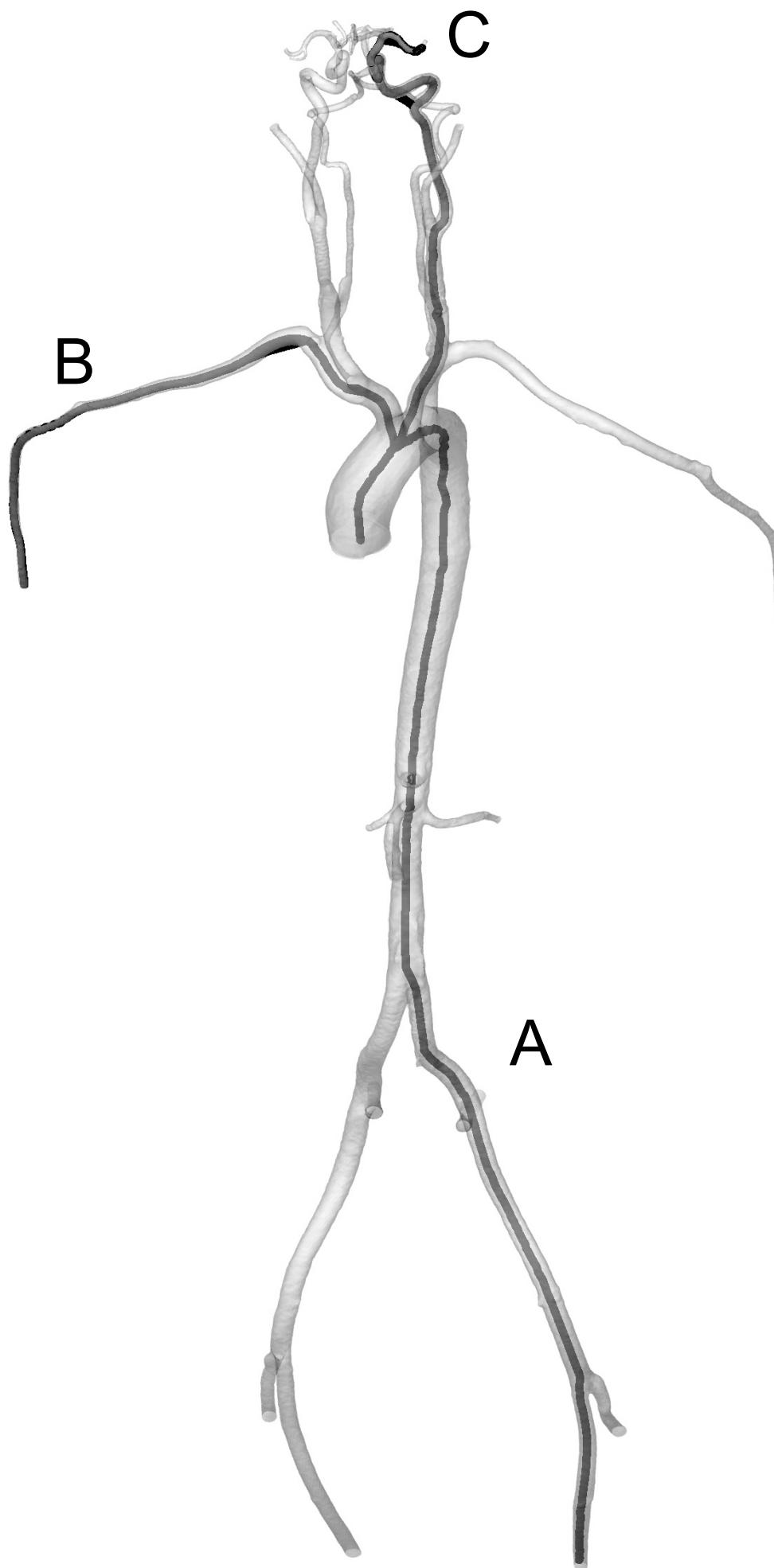
Inlet length



$$\frac{L_e}{D} = 0.064 Re$$

INLET LENGTH. Flow entering a side branch results in skewed profile. It takes a certain inlet length before the velocity develops into a parabolic profile again.

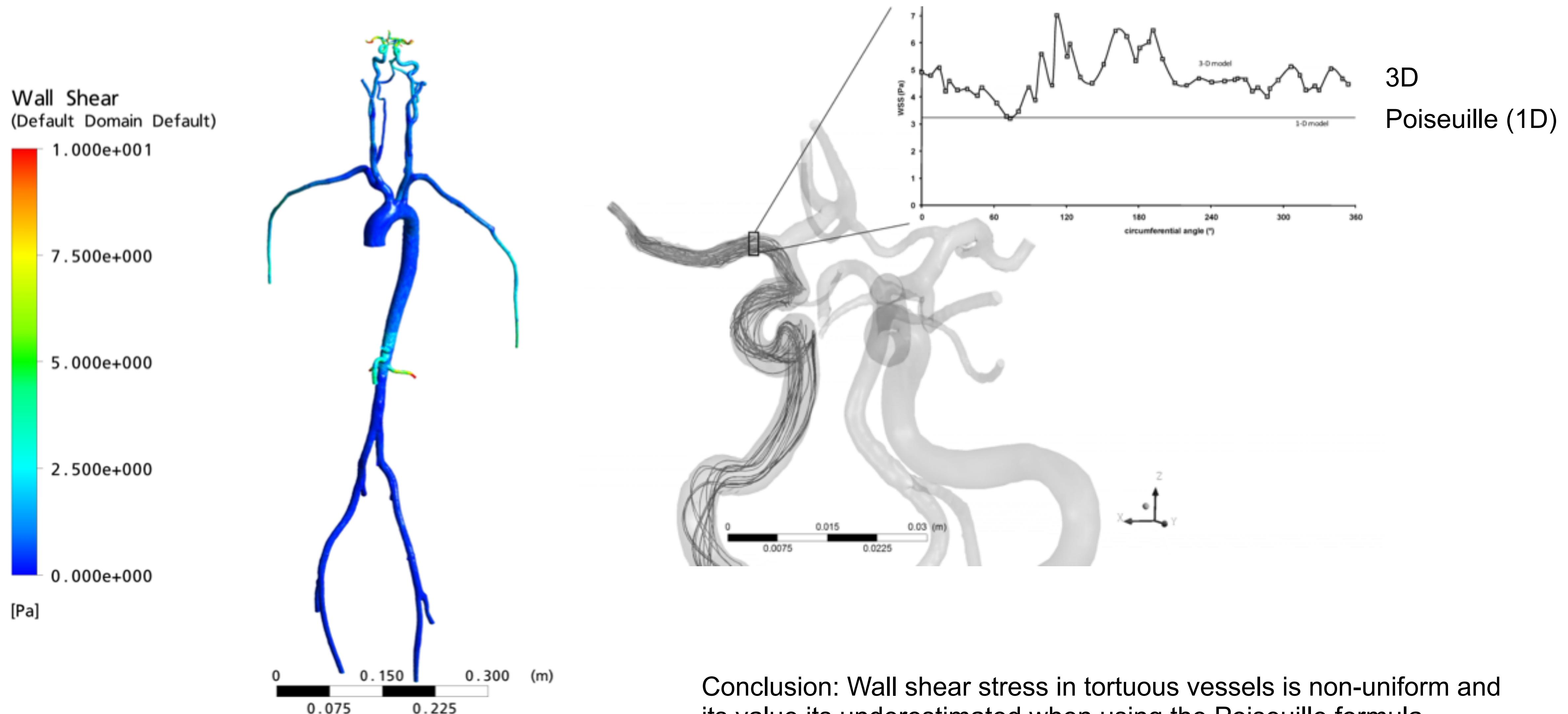
3D and non-Newtonian effects



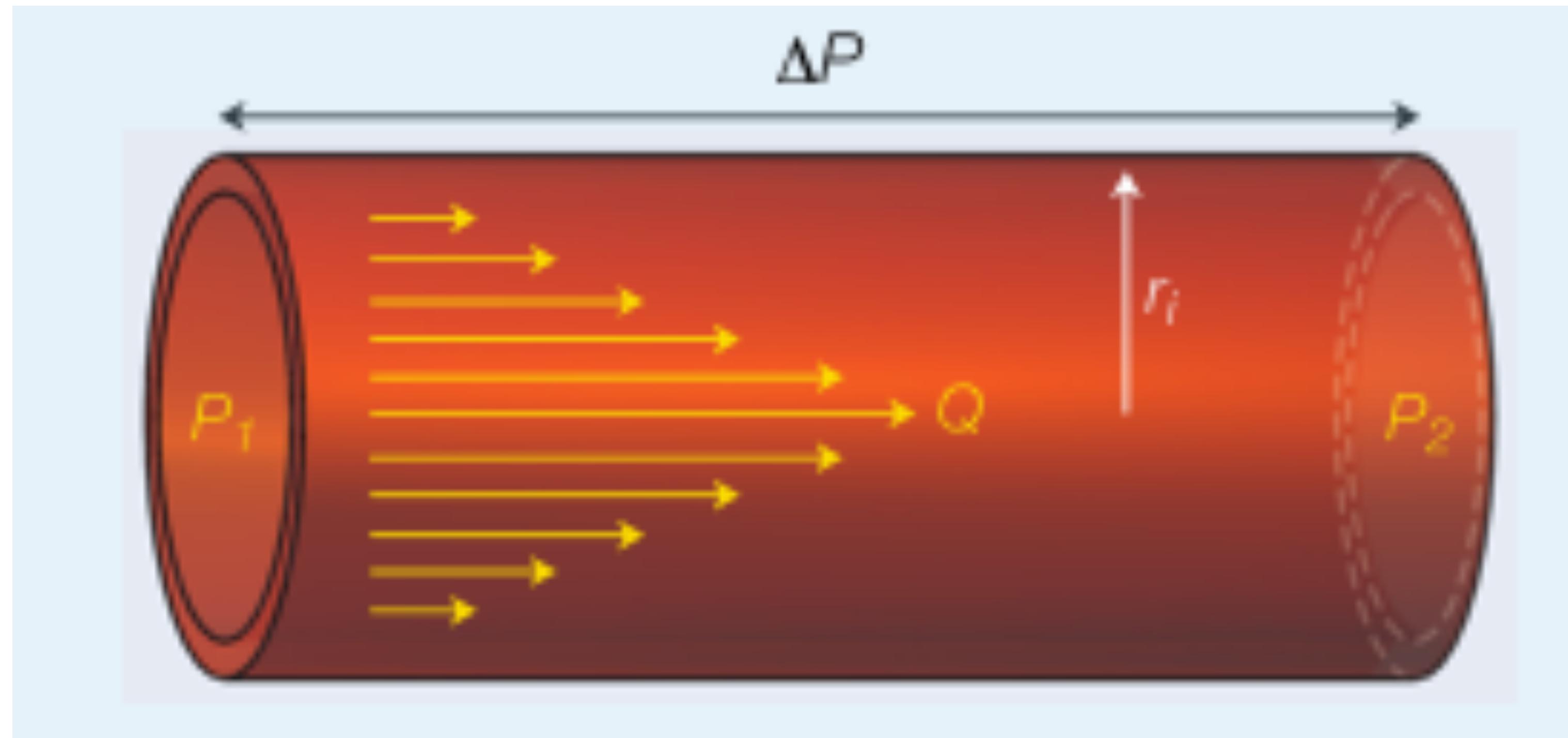
Remarks:

- 1) Non-Newtonian and 3D effects are negligible in the big vessels
- 2) Non-Newtonian and 3D effects are important in small peripheral arteries and in particular in the tortuous vessels of the cerebral circulation

Shear stress distribution

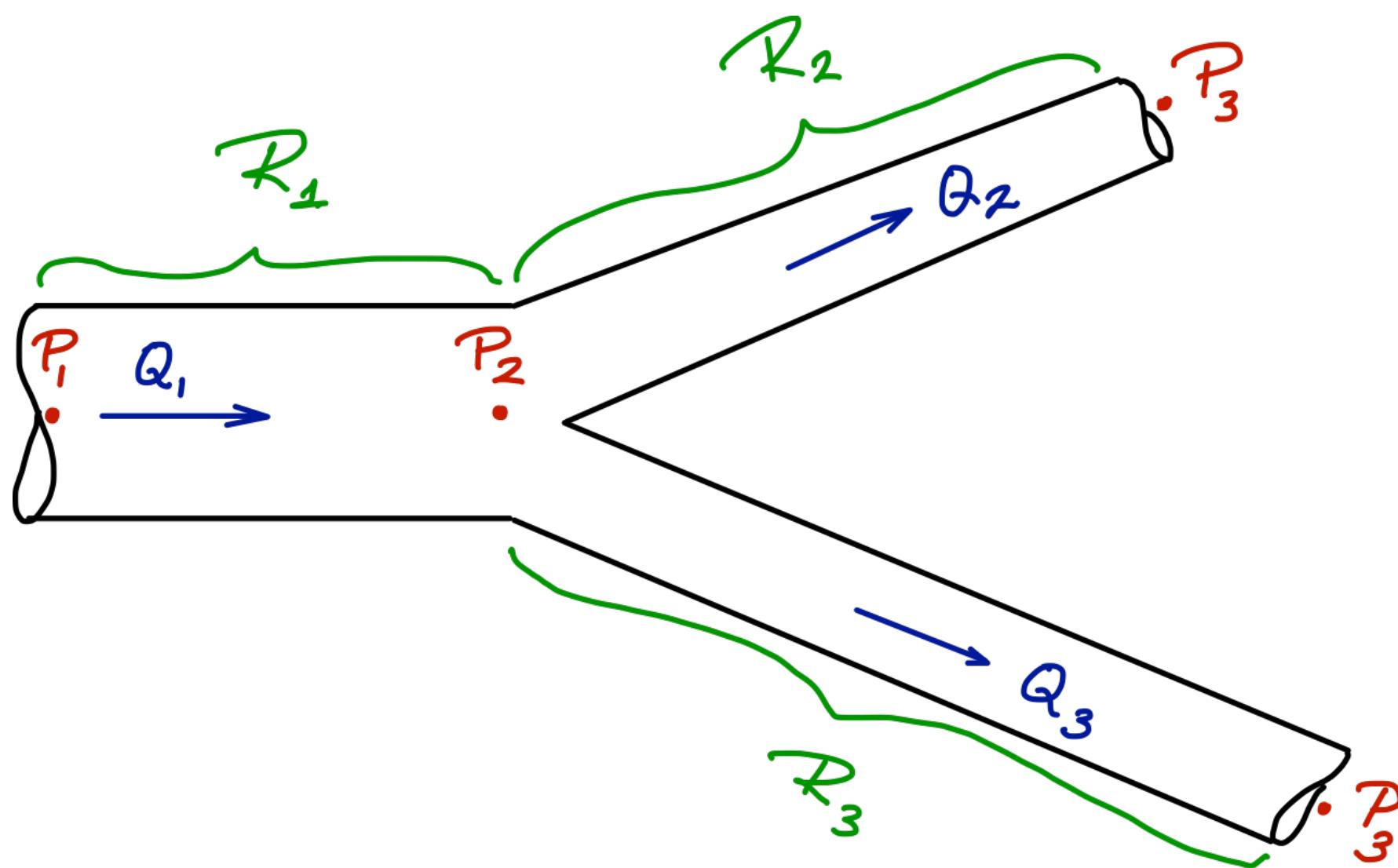


Resistance



$$R = \frac{\Delta P}{Q} = \frac{8\mu l}{\pi r^4}$$

Addition of resistances



Continuity of flow: $Q_1 = Q_2 + Q_3 = \frac{\Delta P_2}{R_2} + \frac{\Delta P_3}{R_3}$

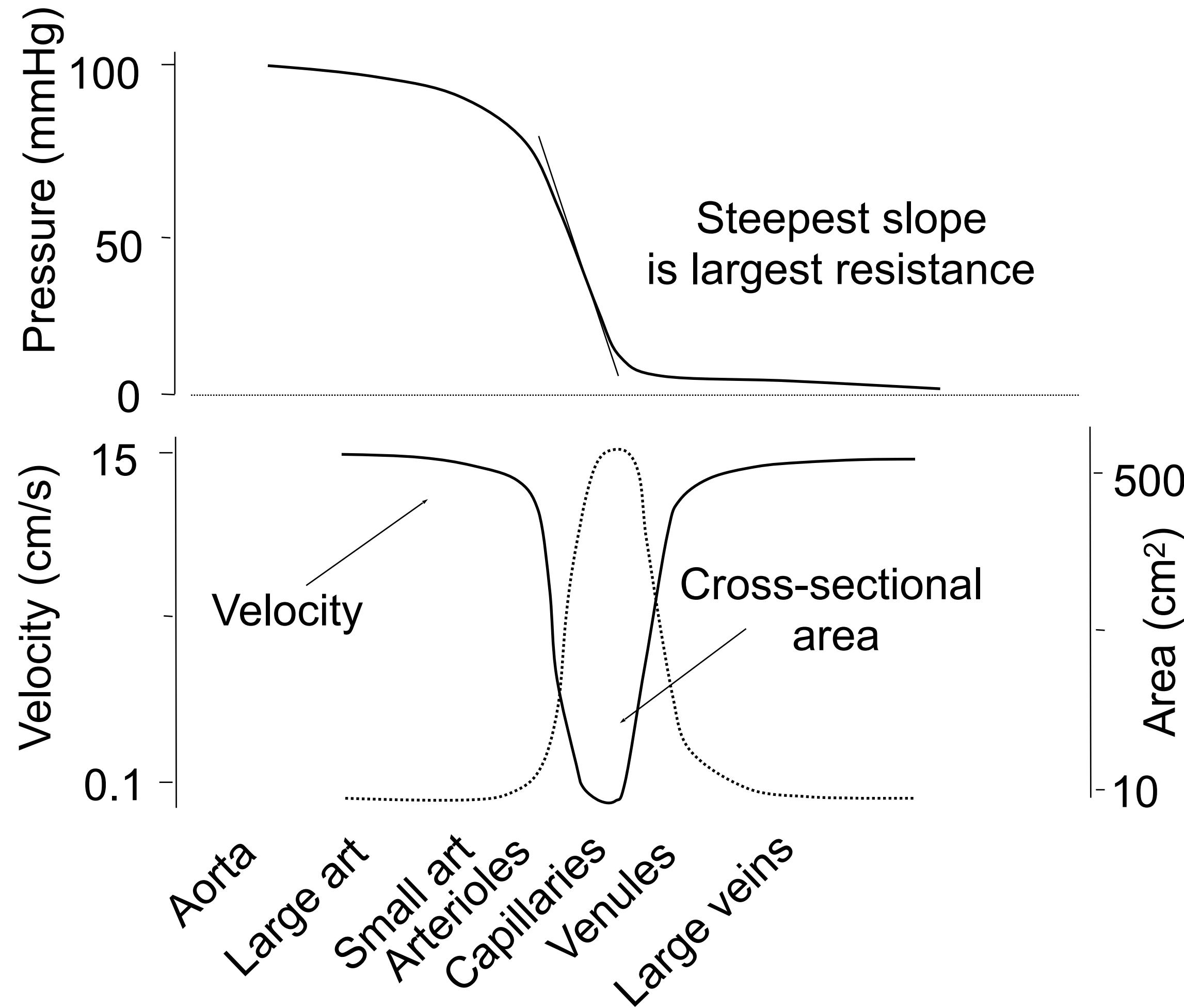
$$\Rightarrow Q_1 = \frac{P_2 - P_3}{R_2} + \frac{P_2 - P_3}{R_3} = (P_2 - P_3) \left(\frac{1}{R_2} + \frac{1}{R_3} \right)$$

$$\Rightarrow \frac{Q_1}{P_2 - P_3} = \frac{1}{R_{2,3}} = \frac{1}{R_2} + \frac{1}{R_3} \quad \text{In parallel (addition of resistances)}$$

$$R_{\text{total}} = \frac{P_1 - P_3}{Q_1} = \underbrace{\frac{P_1 - P_2}{Q_1}}_{R_1} + \underbrace{\frac{P_2 - P_3}{Q_1}}_{R_{2,3}}$$

$$\Rightarrow R_{\text{total}} = R_1 + R_{2,3} \quad \text{In series}$$

Distribution of resistances



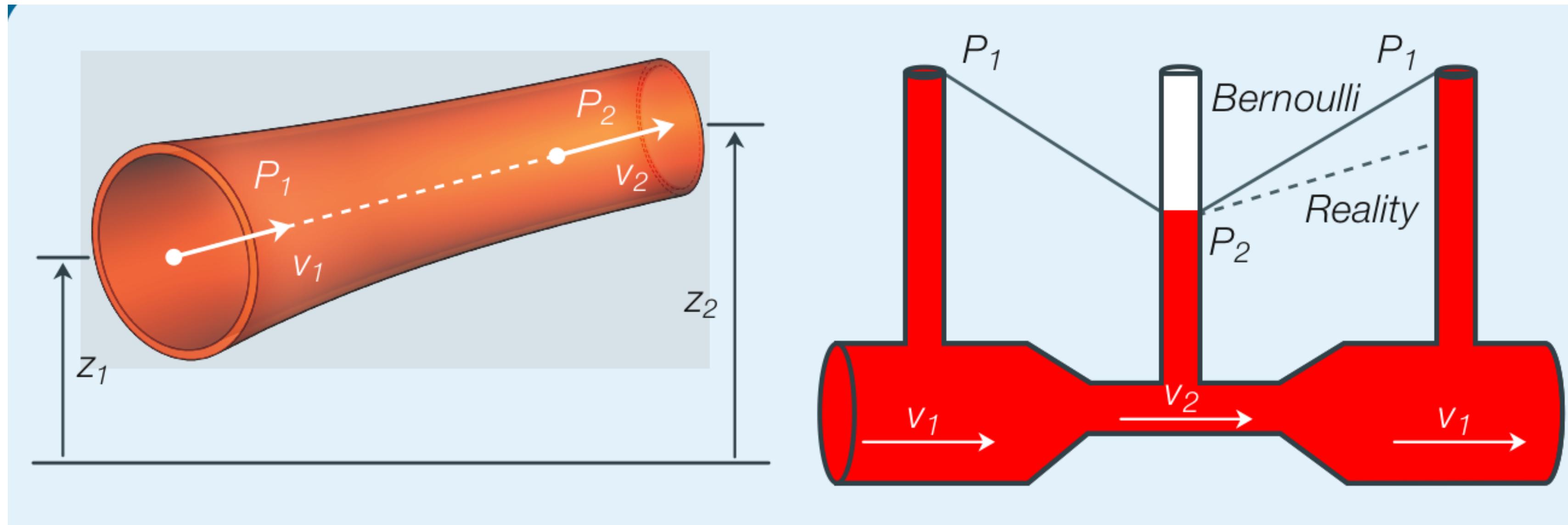
Compare resistances of the aorta, arterioles and capillaries

	Aorta	Arterioles	Capillaries
number of arterial segments in parallel (n)	1	3×10^8	1.5×10^9
Radius (r)	15 mm	7.5 μ	7.5 μ
Length (l)	50 cm	1 mm	1 mm
Resistance of single segment	1.00×10^5	3.22×10^{15}	3.22×10^{15}
$R = \frac{8\mu l}{\pi r^4}$			
Total resistance	1.00×10^5	1.07×10^7	2.14×10^6
$R_{tot} = \frac{R}{n}$			



The highest resistance is at the level of the arterioles

Bernoulli



$$P_1 + \frac{1}{2} \rho v_1^2 + \rho g z_1 = P_2 + \frac{1}{2} \rho v_2^2 + \rho g z_2$$

$$\underbrace{p + \frac{1}{2} \rho V^2}_{\text{Pressure}} + \rho g h = ct$$

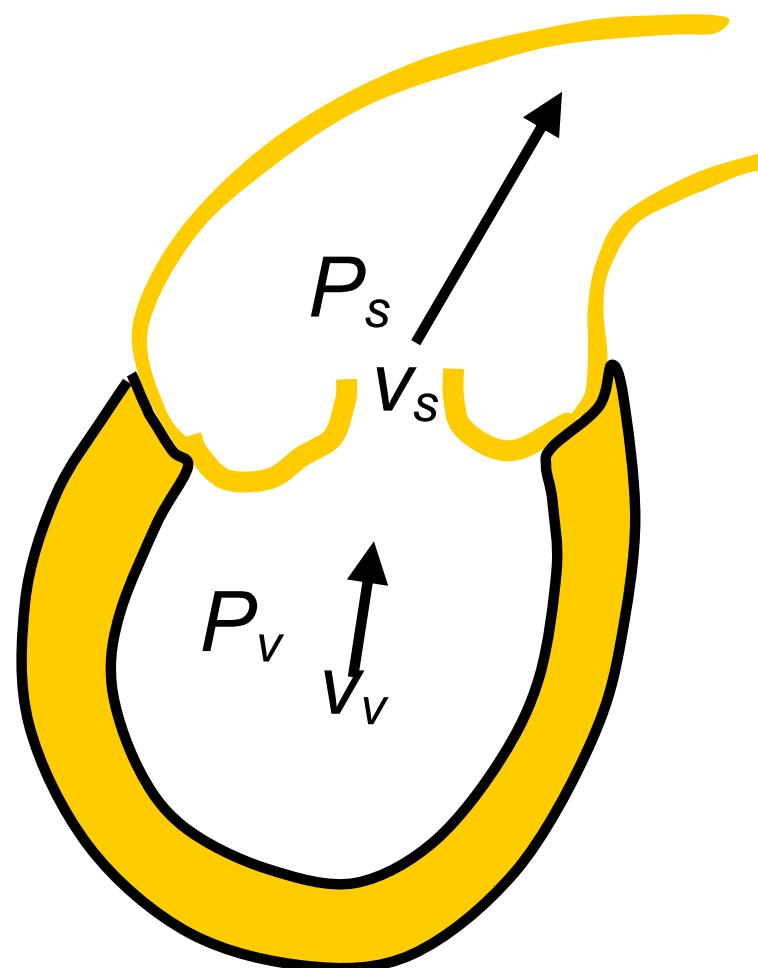
Dynamic Pressure

Hydrostatic Pressure

Conditions:

- No friction (no viscous losses)
- Steady flow
- Along a streamline

Example using the Bernoulli equation: the Gorlin equation for aortic stenosis



Let us consider flow through a stenosed valve according to Figure. Applying Bernoulli's law and assuming height differences can be neglected

$$P_v + \frac{1}{2}\rho V_v^2 = P_s + \frac{1}{2}\rho V_s^2$$

$$\Delta P = P_v - P_s = \frac{1}{2}\rho(V_s^2 - V_v^2)$$

The flow Q is the same at both locations, thus

$$A_v V_v = A_s V_s = Q$$

where A_v and A_s are the cross-sectional areas of ventricle and valve, respectively. Substituting this into the Bernoulli's equation we obtain:

$$\Delta P = P_v - P_s = \frac{1}{2} \rho Q^2 \left(\frac{1}{A_s^2} - \frac{1}{A_v^2} \right)$$

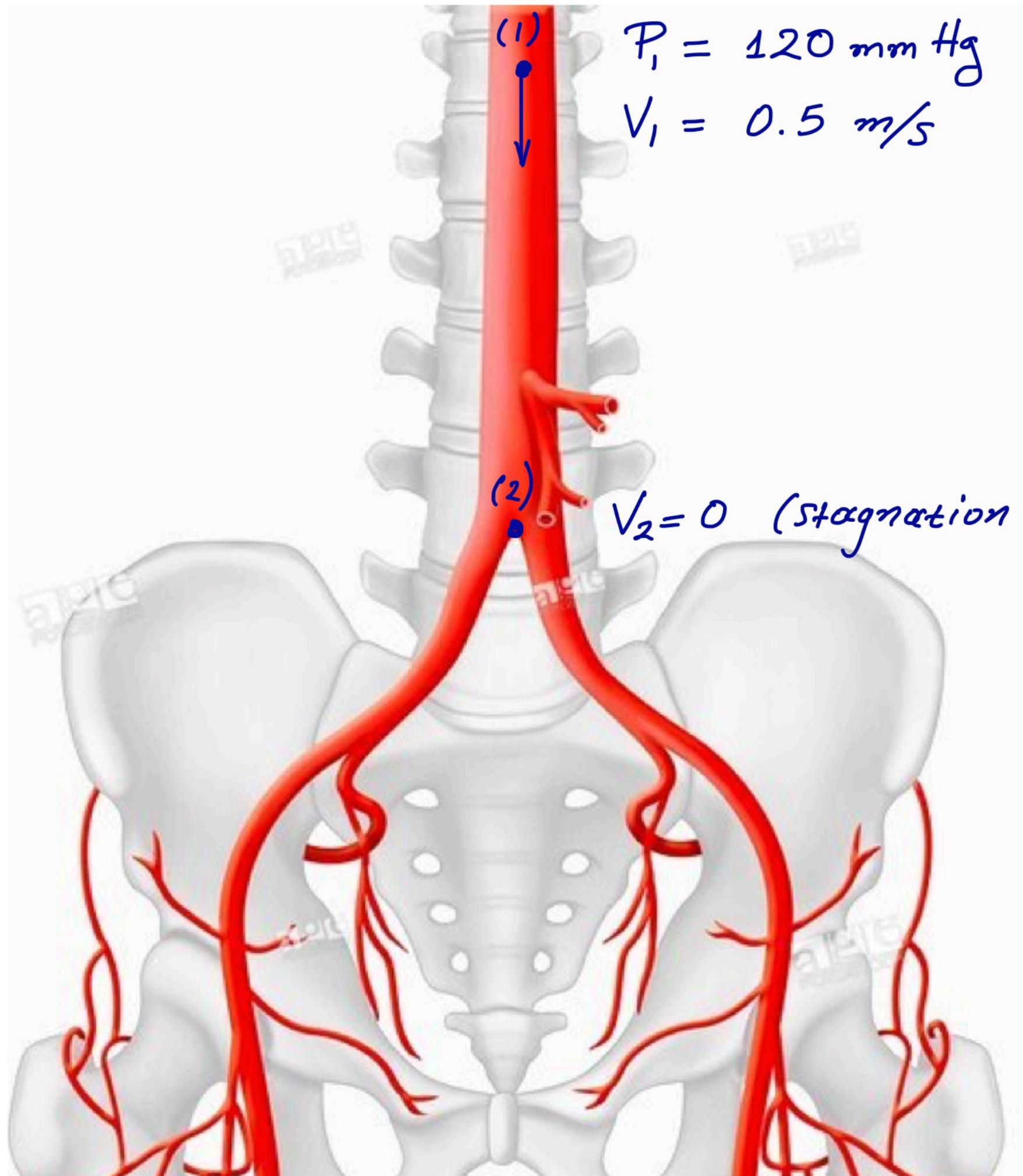
Since $A_s \ll A_v$ the equation can be simplified to:

$$\Delta P = \frac{1}{2} \rho Q^2 / A_s^2 = \frac{1}{2} \rho V_s^2$$

This relation has been used to **estimate effective area**, A_s , of a valvular stenosis by measuring flow and pressure gradient (e.g., using a pressure wire).

$$A_s = Q \sqrt{\frac{\rho}{2 \Delta P}}$$

Example using the Bernoulli equation: pressure rise at the apex of the iliac bifurcation

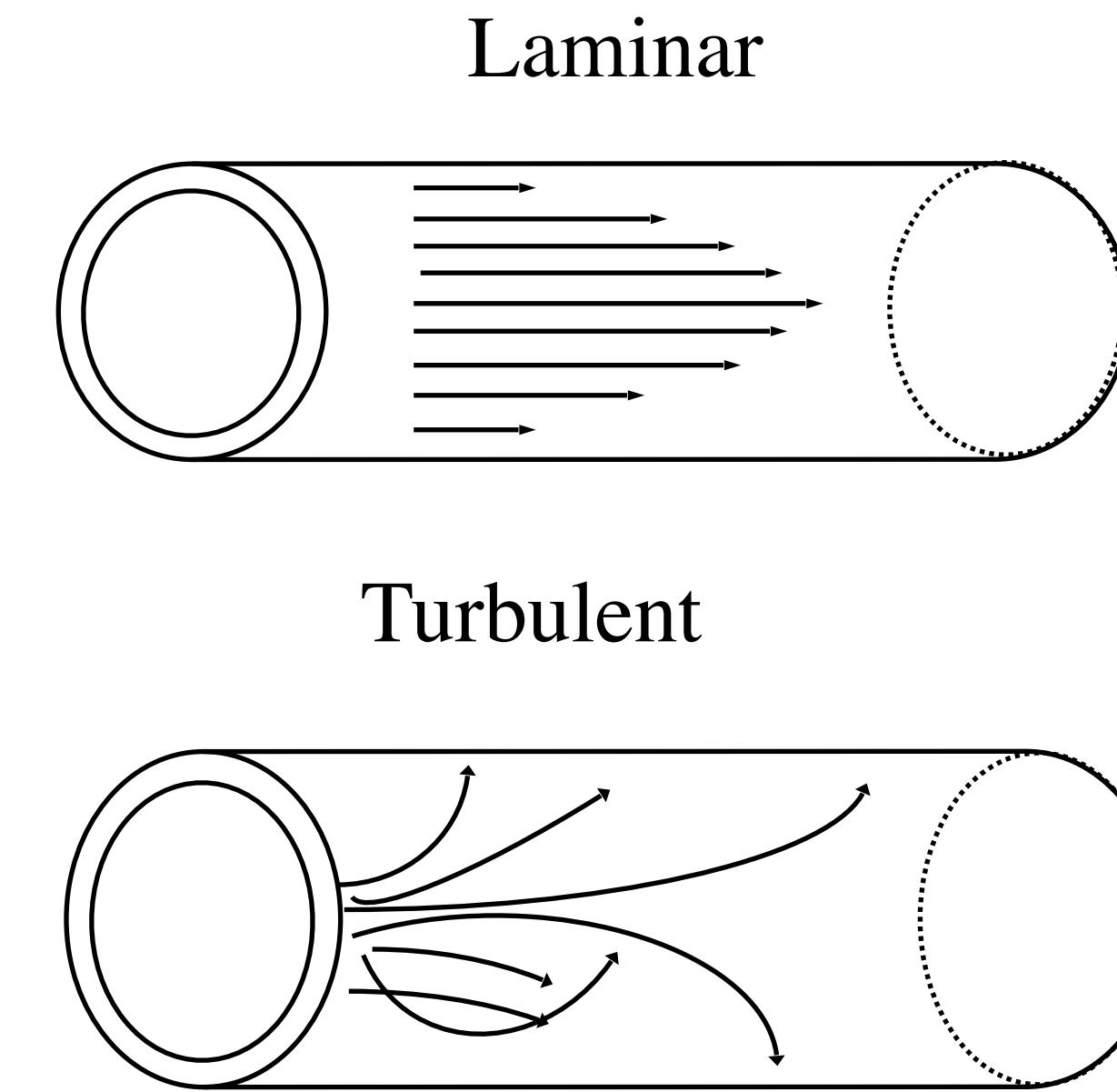
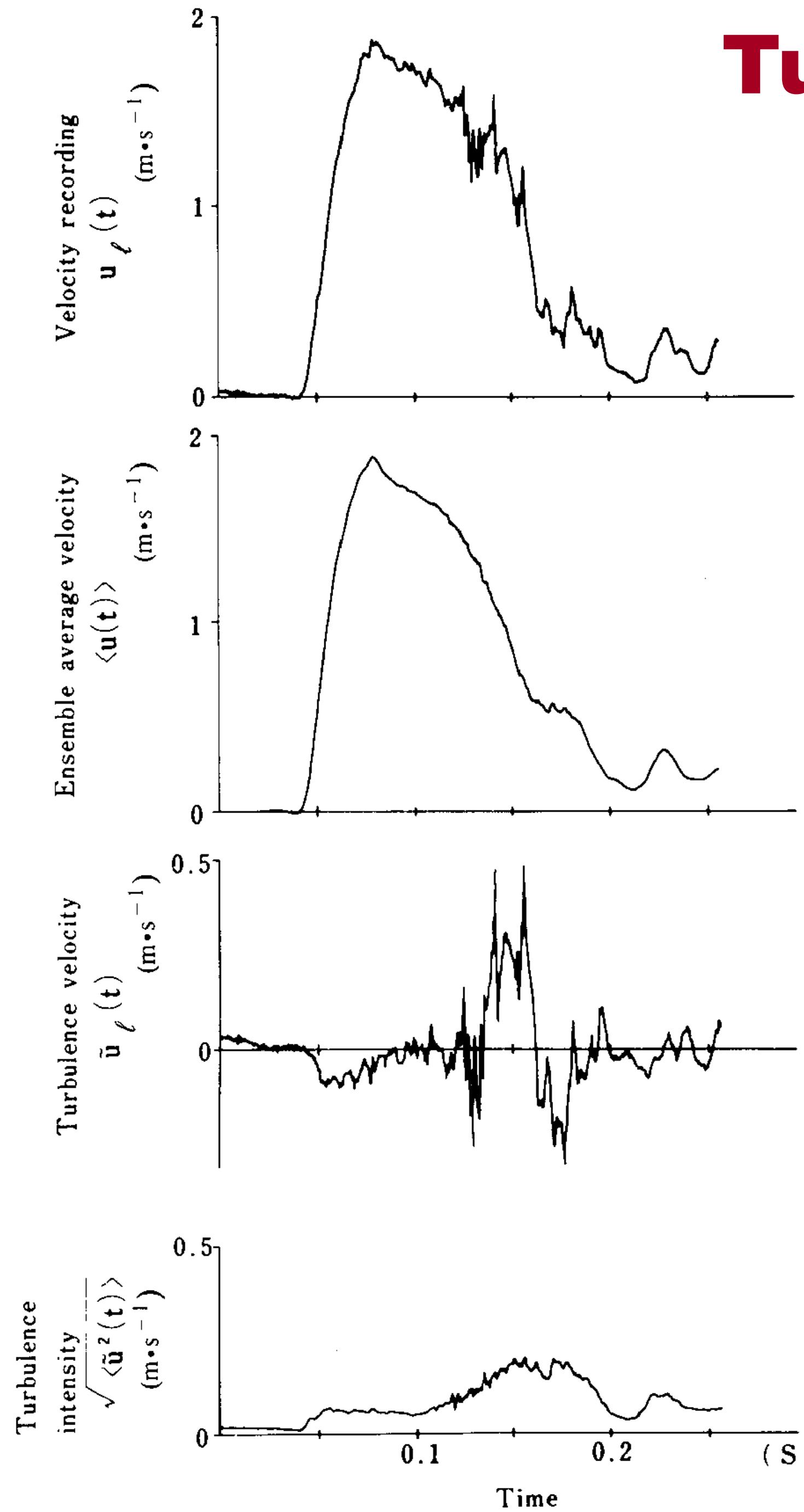


At peak systole ($P = 120 \text{ mmHg}$), the blood flowing in the lower abdominal aorta with a peak velocity $v \approx 0.5 \text{ m/s}$ hits the wall of the apex of the iliac bifurcation.

If it would come to a rest there, velocity is negligible ($v = 0$). On the basis of the Bernoulli equation

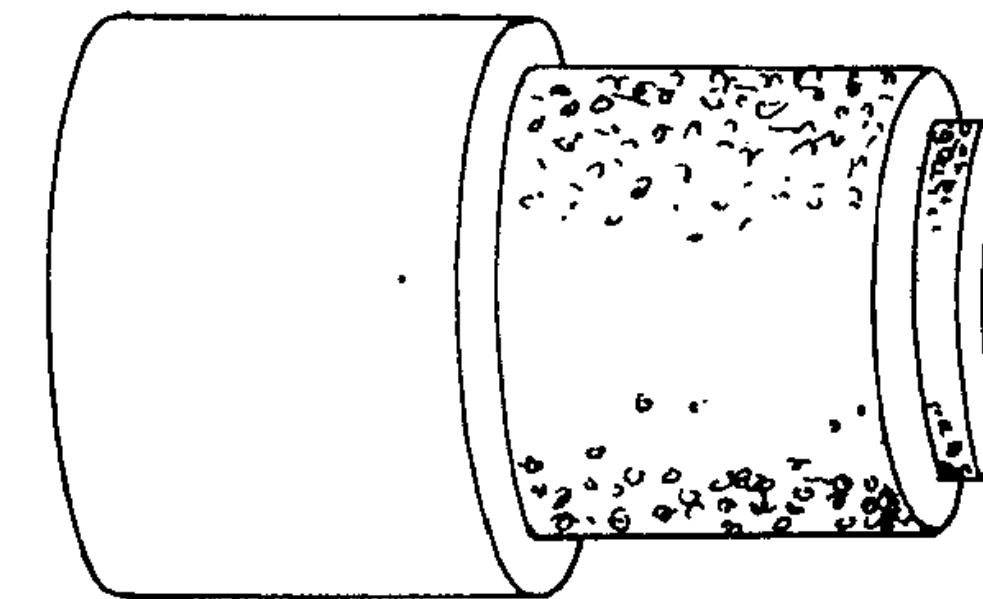
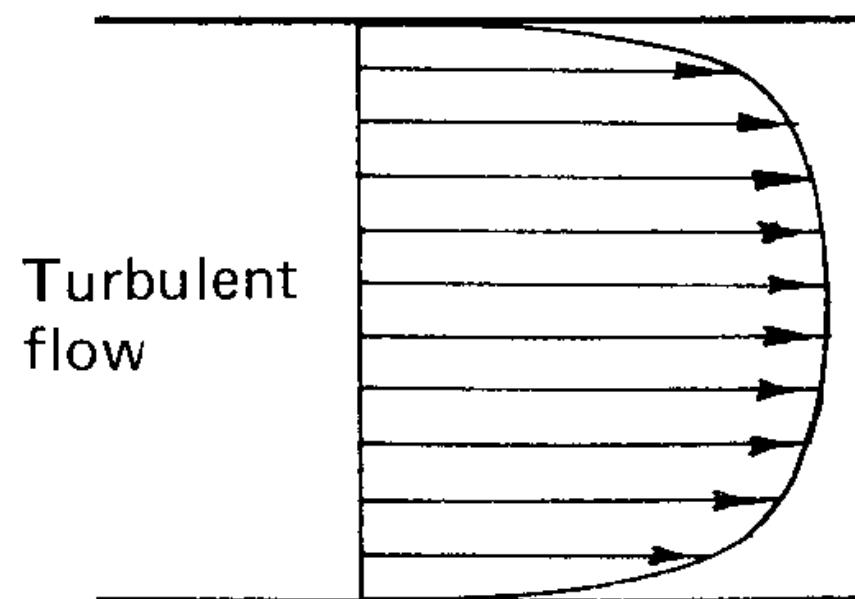
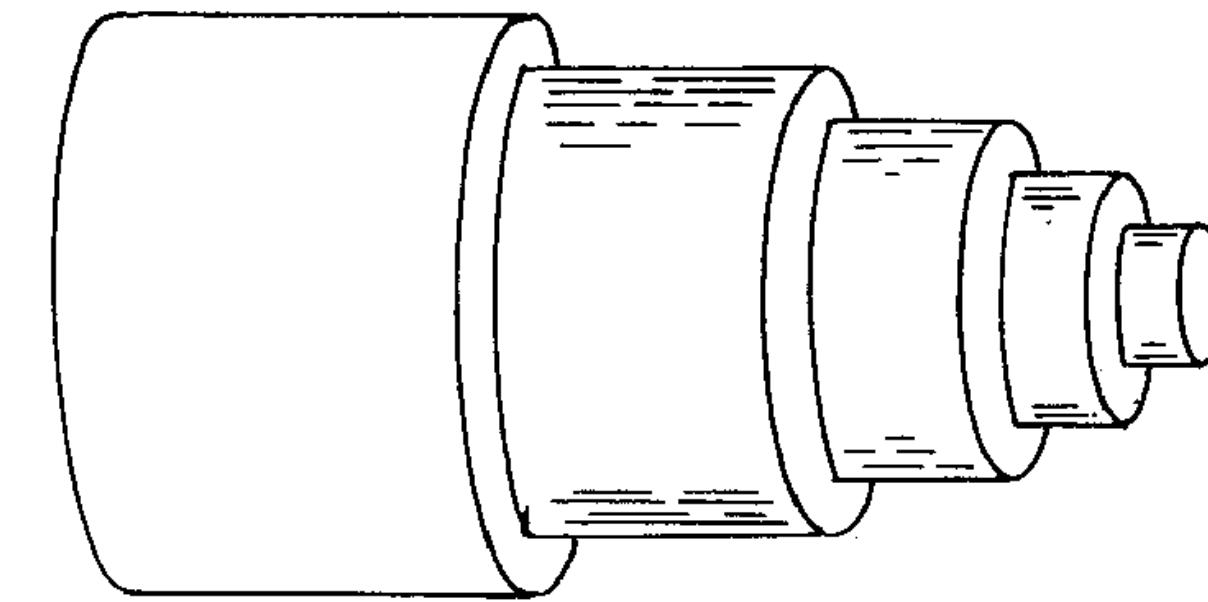
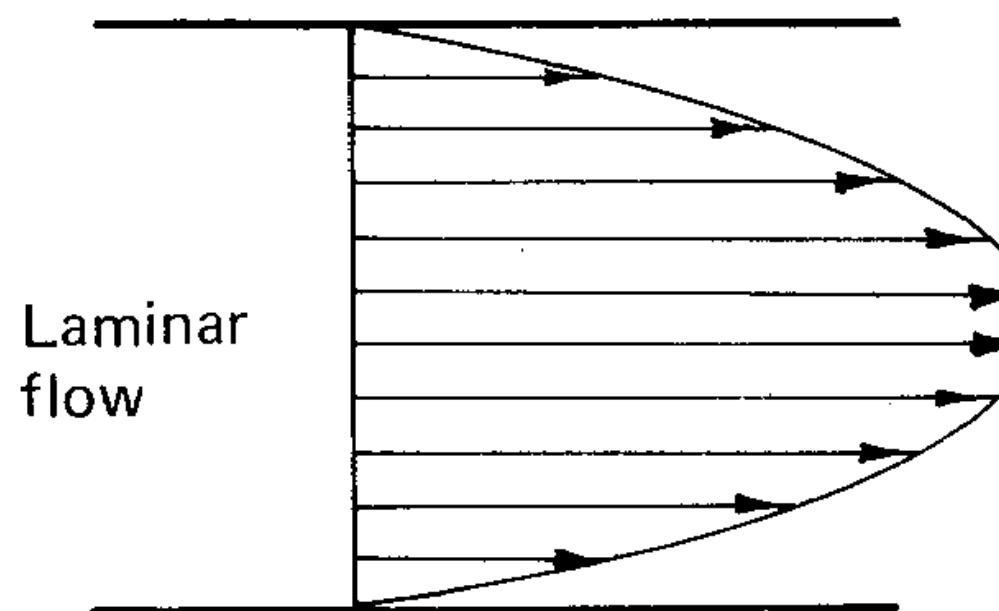
$$\begin{aligned}
 P_1 + \frac{1}{2} \rho V_1^2 &= P_2 + \frac{1}{2} \rho V_2^2 \\
 \Rightarrow P_2 &= P_1 + \frac{1}{2} \rho V_1^2 = 120 \text{ mmHg} + \frac{1}{2} \cdot 1060 \frac{\text{kg}}{\text{m}^3} \cdot 0.5^2 \frac{\text{m}^2}{\text{s}^2} \\
 &= 120 \text{ mmHg} + 132 \text{ Pa} \cdot \left(\frac{1 \text{ mmHg}}{133 \text{ Pa}} \right) \\
 &= 120 \text{ mmHg} + \underline{\underline{1 \text{ mmHg}}} \\
 &\quad \text{Pressure rise}
 \end{aligned}$$

Turbulence



- “Random”, erratic movement of fluid particles
- Energy dissipation
- Increased friction:
 $\tau = \mu \cdot \text{“shear rate”}$

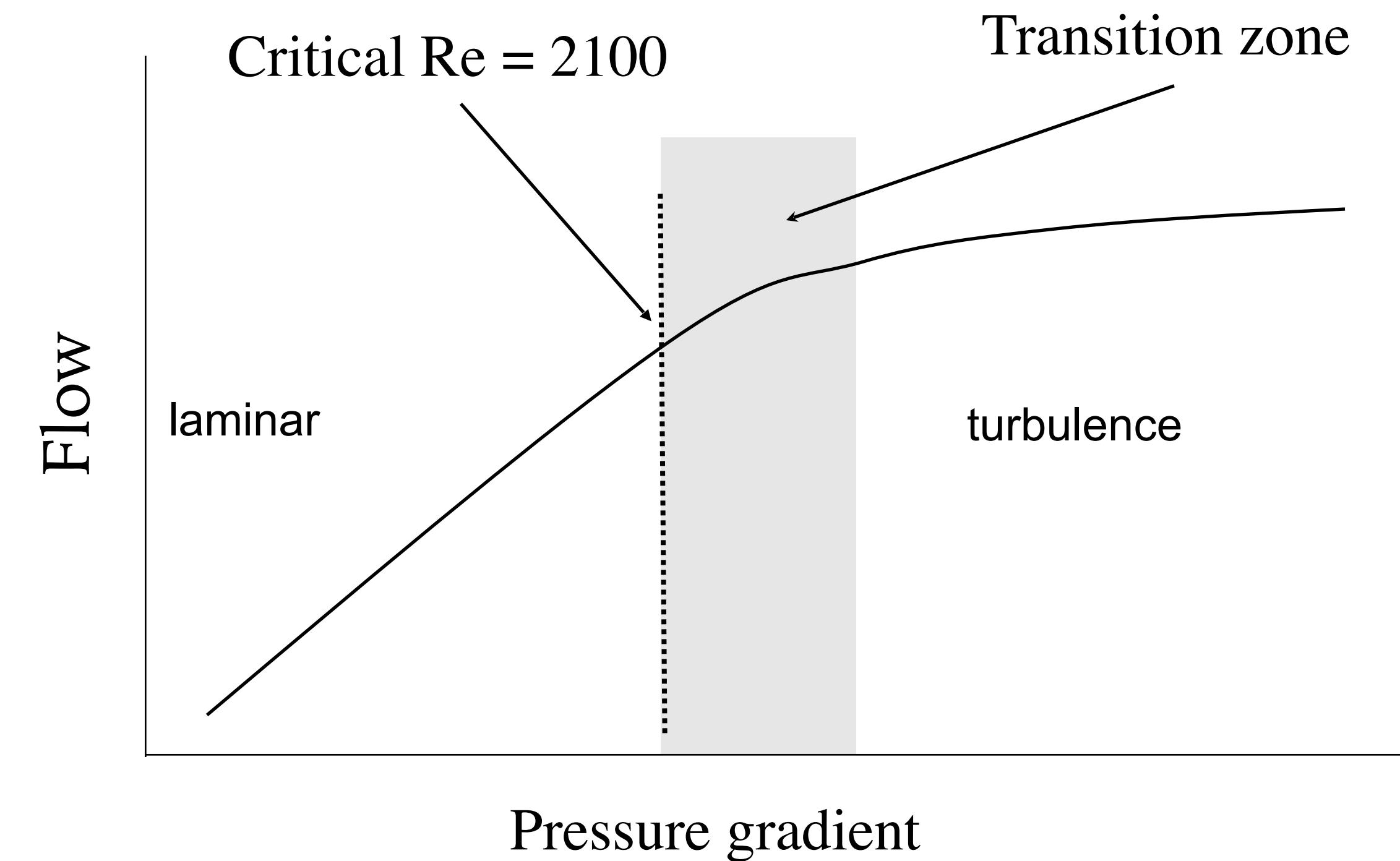
Turbulence: velocity profile



Velocity profile

Sliding shell analog

Reynolds number and transition to turbulence



Reynolds number

$$Re = \frac{\rho D V}{\mu} = \frac{\text{Inertial effects}}{\text{Viscous effects}}$$